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(REV. 11-94)

U.S. DEPARTMENT OF COMMERCE  
PATENT AND TRADEMARK OFFICE

ATTORNEY'S DOCKET NUMBER

1803-334-999

**TRANSMITTAL LETTER TO THE UNITED STATES  
DESIGNATED/ELECTED OFFICE (DO/EO/US)**

**10/070343**

INTERNATIONAL APPLICATION NO.  
PCT/EP00/08587

INTERNATIONAL FILING DATE  
2 September 2000

PRIORITY DATE CLAIMED  
4 September 1999

TITLE OF INVENTION  
SYSTEM FOR THERMOCYCLING OF FLUIDS IN CARTRIDGES

APPLICANT(S) FOR DO/EO/US  
Urban Schnell, Olivier Elsenhans, Thomas Caratsch, Lukas Birrer and Ernad Saroth

Applicant herewith submits to the United States Designated/ Elected Office (DO/EO/US) the following items under 35 U.S.C. 371:

1. ☒ This is a **FIRST** submission of items concerning a filing under 35 U.S.C. 371.
2. ☐ This is a **SECOND** or **SUBSEQUENT** submission of items concerning a filing under 35 U.S.C. 371.
3. ☒ This express request to begin national examination procedures (35 U.S.C. 371(f)) at any time rather than delay examination until the expiration of the applicable time limit set in 35 U.S.C. 371(b) and PCT Articles 22 and 39(1).
4. ☒ A proper Demand for International Preliminary Examination was made by the 19th month from the earliest claimed priority date.
5. ☒ A copy of the International Application as filed (35 U.S.C. 371(c)(2))
  - a. ☒ is transmitted herewith (required only if not transmitted by the international Bureau).
  - b. ☐ has been transmitted by the International Bureau.
  - c. ☐ is not required, as the application was filed in the United States Receiving Office (RO/US)
6. ☐ A translation of the International Application into English (35 U.S.C. 371(c)(2)).
7. ☒ Amendments to the claims of the International Application under PCT Article 19 (35 U.S.C. 371(c)(3))
  - a. ☒ are transmitted herewith (required only if not transmitted by the International Bureau).
  - b. ☒ have been transmitted by the International Bureau.
  - c. ☐ have not been made; however, the time limit for making such amendments has NOT expired.
  - d. ☐ have not been made and will not be made.
8. ☐ A translation of the amendments to the claims under PCT Article 19 (35 U.S.C. 371(c)(3)).
9. ☒ An oath or declaration of the inventor(s) (35 U.S.C. 371(c)(4)) (unexecuted).
10. ☐ A translation of the annexes to the International Preliminary Examination Report under PCT Article 36 (35 U.S.C. 371(c)(5)).

**Items 11. to 16. below concern document(s) or information included:**

11. ☐ An Information Disclosure Statement under 37 CFR 1.97 and 1.98.
12. ☐ An assignment document.
13. ☒ A **FIRST** preliminary amendment.  
☐ A **SECOND** or **SUBSEQUENT** preliminary amendment.
14. ☐ A substitute specification (clean copy and marked up copy).
15. ☐ A change of power of attorney and/or address letter.
16. ☒ Other items or information: Please enter the First Preliminary Amendment filed herewith prior to calculation of any fees.

10/070343

- 17.
- ☒
- The U.S. National Fee (35 U.S.C. 371(c)(1)) and other fees as follows:

## CLAIMS

(1)FOR	(2)NUMBER FILED	(3)NUMBER EXTRA	(4)RATE	(5)CALCULATIONS
TOTAL CLAIMS	28 - 20	8	X \$ 18.00	\$ 144.00
INDEPENDENT CLAIMS	2 - 3	0	X \$ 84.00	0.00
MULTIPLE DEPENDENT CLAIM(S) (if applicable)			+ \$ 280.00	280.00

BASIC NATIONAL FEE (37 CFR 1.492(a)(1)-(5)):

**CHECK ONE BOX ONLY**

<input type="checkbox"/> International preliminary examination fee paid to USPTO (37 CFR 1.482) .....	\$ 710
<input type="checkbox"/> No international preliminary examination fee paid to USPTO (37 CFR 1.482) but international search fee paid to USPTO (37 CFR 1.445(a)(2)) .....	\$ 740
<input type="checkbox"/> Neither international preliminary examination fee (37 CFR 1.482) nor international search fee (37 CFR 1.445(a)(2)) paid to USPTO .....	\$ 1040
<input type="checkbox"/> International preliminary examination fee paid to USPTO (37 CFR 1.482) and all claims satisfied provisions of PCT Article 33(2) to (4) .....	\$ 100
<input checked="" type="checkbox"/> Filing with EPO or JPO search report .....	\$ 890
Surcharge of \$130.00 for furnishing the National fee or oath or declaration later than 20 or 30 mos. from the earliest claimed priority date (37 CFR 1.492(e)).	
TOTAL OF ABOVE CALCULATIONS	= 1,314.00
Reduction by 1/2 for filing by small entity, if applicable. Affidavit must be filed also. (Note 37 CFR 1.9, 1.27, 1.28).	- \$
SUBTOTAL	= 1,314.00
Processing fee of \$130.00 for furnishing the English Translation later than 20 30 mos. from the earliest claimed priority date (37 CFR 1.492(f)).	+
0 TOTAL FEES ENCLOSED	\$ 1,314.00

- a. ☐ A check in the amount of \$ \_ to cover the above fees is enclosed.
- b. ☒ Please charge Deposit Account No. 16-1150 in the amount of \$ 1,314.00 to cover the above fees. A copy of this sheet is enclosed.
- c. ☒ The Commissioner is hereby authorized to charge any additional fees which may be required, or credit any overpayment to Deposit Account No. 16-1150. A copy of this sheet is enclosed.
18. ☐ Other instructions  
Please enter the preliminary amendment before calculating the fee.
19. ☒ All correspondence for this application should be mailed to  
PENNIE & EDMONDS LLP  
1155 AVENUE OF THE AMERICAS  
NEW YORK, NEW YORK 10036-2711
20. ☒ All telephone inquiries should be made to (212) 790-2803

Rahul Pathak

NAME

For: Jennifer Gordon

(Reg. No. 30,753)

SIGNATURE

42,983

REGISTRATION NUMBER

February 28, 2002

DATE

Express Mail No.: EL 452 482 539 US

**IN THE UNITED STATES PATENT AND TRADEMARK OFFICE**

Application of: Schnell *et al.*

Serial No.: Unassigned

Group Art Unit: Unassigned

Filed: Herewith

Examiner: Unassigned

For: SYSTEM FOR  
THERMOCYCLING OF FLUIDS  
IN CARTRIDGES

Attorney Docket No.:  
1803-334-999

**PRELIMINARY AMENDMENT UNDER 37 C.F.R. §1.111**

Assistant Commissioner for Patents  
Washington, D.C. 20231

Sir:

In accordance with Rule 111 of the Rules of Practice, please consider and enter the following amendments and remarks.

**AMENDMENTS**

**IN THE CLAIMS:**

A marked-up copy of the following amended claims is attached as Exhibit A.

Please amend Claims 1-24 to read as follows:

1. (Amended) A system for thermocycling of fluids in cartridges comprising
  - a) a cartridge with at least one heat conducting wall and at least one light transparent wall, the cartridge having a fluid inlet and an outlet which are connected by a channel,

said cartridge having a protrusion such that the channel is longer than the shortest distance between the fluid inlet and fluid outlet to allow bubble-free flow-through filling of the cartridge,

- b) a thermocycling unit in thermal contact with said heat conducting wall of said cartridge,
  - c) a light source for transmitting light into the interior of said cartridge through said light transparent wall of said cartridge which is arranged substantially perpendicular to said heat conducting wall,
  - d) a light detector for detecting light emerging from the interior of the cartridge through said light transparent wall,
  - e) a fluid providing unit coupled to an inlet of the cartridge for providing the cartridge with fluid by flow-through-filling.
2. (Amended) The system of claim 1, wherein the cartridge has a body comprising the light transparent wall and having at least one opening which is sealed by a foil providing said heat conducting wall.
3. (Amended) The system of claim 2, wherein the body is a frame which is sealed by two foils providing heat conducting walls.
4. (Amended) The system of claim 1 for conducting fluorescent measurements wherein the light detector detects fluorescent light emerging from the cartridge.
5. (Amended) The system of claim 1, wherein the thermocycling unit comprises at least one plate in thermal contact with the heat conducting wall of the cartridge.

6. (Amended) The system of claim 1, wherein the cartridge is wedge shaped and the thermocycling unit comprises a wedge shaped receiving section for receiving said wedge shaped cartridge.
7. (Amended) The system of claim 6, wherein the opposing walls forming the wedge shaped cartridge comprise opposing walls having an angle of 3 to 8° one to another.
8. (Amended) The system of claim 1, wherein said light transparent wall comprises a first section through which light is passed from the light source into the cartridge and a second section through which light is passed from the interior of the cartridge onto the light detector.
9. (Amended) The system of claim 8, wherein said first section is tilted with respect to the illumination beam axis so that the light is refracted towards the second section of said transparent wall.
10. (Amended) The system of claim 1 or 5, wherein said thermocycling unit comprises a plate in thermal contact with said heat conducting wall of the cartridge and which exerts pressure onto said wall.
11. (Amended) The system of claim 1, wherein the quotient of the maximal width of said channel and the depth of said channel is in the range of 1 to 10.
12. (Amended) The system of claim 1 or 11, wherein the depth of the channel is in the range of 0.5 to 5 mm.
13. (Amended) A cartridge for conducting thermal cycling of fluids, comprising
  - a) a substantially planar and heat conducting wall,

- b) a light transparent wall which is disposed substantially vertical to said heat conducting wall,
  - c) an fluid inlet for providing the cartridge with fluid,
  - d) an fluid outlet for draining fluid or gas from the cartridge,
  - e) a channel connecting inlet and outlet wherein said cartridge having a protrusion such that the channel between fluid inlet and fluid outlet is longer than the shortest distance between fluid inlet and fluid outlet to allow flow-through-filling of the cartridge to avoid bubbles in a measuring section of the cartridge.
14. (Amended) The cartridge of claim 13, having two opposing heat conducting walls.
15. (Amended) The cartridge of claim 13 or 14, wherein the heat conducting wall is a foil with a thickness of less than 200µm.
16. (Amended) The cartridge of claim 13 or 14, having two opposing walls from which at least one is a heat conducting wall and which form an angle of 3 to 8° with respect to each other.
17. (Amended) The cartridge of claim 13, wherein the light transparent wall comprises a first section for transmitting light into the cartridge and a second section for transmitting light emerging from the cartridge.
18. (Amended) The cartridge of claim 13, which is made from a body having at least one opening which is closed by a heat conducting foil.
19. (Amended) The cartridge of claim 13, which is made from a frame which is closed by two opposing foils.

20. (Amended) The cartridge of claim 13 having a thickness of 0.5 to 5 mm.
21. (Amended) The cartridge of claim 13, wherein the quotient of the maximal width of said channel and the depth of said channel is in the range of 1 to 10.
22. (Amended) The cartridge of claim 21, wherein the depth of the channel is in the range of 0.5 to 5 mm.
23. (Amended) A method for thermocycling of fluids employing a system according to claim 1, comprising the steps of
- filling the cartridge by a flow-through-process avoiding bubbles in a measuring section of the cartridge,
  - thermal cycling of fluid in the cartridge,
  - transmitting light into the cartridge and
  - detecting light emerging the cartridge.
24. (Amended) The method of claim 23 additionally comprising monitoring the light emerging the cartridge to monitor amplification of nucleic acids in the fluid during thermal cycling.

**REMARKS**

Claims 1-24 are pending and under consideration in the instant application. With the instant Amendment, Claims 1-24 are amended. For the PTO's convenience, a clean copy of pending Claims 1-24 after entry of the instant Amendment is attached hereto as Exhibit B.

Applicants expressly reserve the right to pursue any canceled subject matter in one or more related, continuation, divisional or continuation-in-part application(s).

**THE AMENDMENT OF THE CLAIMS**


Claims 1-24 have been amended to conform them with current U.S. practice. As the amendments to the claims are fully supported by the specification and claims as originally filed, they do not constitute new matter. Entry thereof is therefore respectfully requested.

**CONCLUSION**

No fees are believed due in connection with this response. However, the Commissioner is authorized to charge all required fees, fees under 37 CFR § 1.17 and all required extension of time fees, or credit any overpayment, to Pennie & Edmonds U.S. Deposit Account No. 16-1150.

Respectfully submitted,

Date: February 28, 2002

  
Rahul Pathak 42983  
(Reg. No.)

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Enclosure (Exhibits A&B)



**Exhibit A**  
**Marked-Up Version of Amended Claims**

1. (Amended) [System] A system for thermocycling of fluids in cartridges comprising
  - a) a cartridge with at least one heat conducting wall and at least one light transparent wall, the cartridge having a fluid inlet and an outlet which are connected by a channel,

said cartridge having a protrusion [(5)] such that the channel is longer than the shortest distance [(D)] between the fluid inlet and fluid outlet to allow bubble-free flow-through filling of the cartridge,
  - b) a thermocycling unit in thermal contact with said heat conducting wall of said cartridge [(1)],
  - c) a light source [(30)] for transmitting light into the interior of said cartridge through said light transparent wall of said cartridge which is arranged substantially perpendicular to said heat conducting wall,
  - d) a light detector [(20)] for detecting light emerging from the interior of the cartridge through said light transparent wall,
  - e) a fluid providing unit coupled to an inlet of the cartridge for providing the cartridge with fluid by flow-through-filling.
2. (Amended) [System according to] The system of claim 1, wherein the cartridge has a body comprising the light transparent wall and having at least one opening which is sealed by a foil providing said heat conducting wall.
3. (Amended) [System according to] The system of claim 2, wherein the body is a frame which is sealed by two foils providing heat conducting walls.

4. (Amended) [System according to] The system of claim 1 for conducting fluorescent measurements wherein the light detector detects fluorescent light emerging from the cartridge.
5. (Amended) [System according to] The system of claim 1, wherein the thermocycling unit comprises at least one plate [(40)] in thermal contact with the heat conducting wall of the cartridge.
6. (Amended) [System according to] The system of claim 1, wherein the cartridge is wedge shaped and the thermocycling unit [comprising] comprises a wedge shaped receiving section for receiving said wedge shaped cartridge.
7. (Amended) [System according to] The system of claim 6, [where] wherein the opposing walls forming the wedge shaped cartridge comprise opposing walls having an angle of 3 to 8° one to another.
8. (Amended) [System according to] The system of claim 1, wherein said light transparent wall comprises a first section through which light is passed from the light source into the cartridge and a second section through which light is passed from the interior of the cartridge onto the light detector.
9. (Amended) [System according to] The system of claim 8, wherein said first section is tilted with respect to the illumination beam axis so that the light is refracted towards the second section of said transparent wall.
10. (Amended) [System according to] The system of claim 1 or 5, wherein said thermocycling unit comprises a plate [(40)] in thermal contact with said heat conducting wall of the cartridge and which exerts pressure onto said wall.
11. (Amended) [System according to] The system of claim 1, wherein [said channel has a width DL (lateral diameter) and a depth DV (vertical diameter) and wherein] the quotient of

the maximal width [DL, max] of said channel and [DV] the depth of said channel is in the range of 1 to 10.

12. (Amended) [System according to] The system of claim 1 or 11, wherein the depth [DV (vertical diameter)] of the channel is in the range of 0.5 to 5 mm.

13. (Amended) [Cartridge] A cartridge for conducting thermal cycling of fluids, comprising

- a) a substantially planar and heat conducting wall,
- b) a light transparent wall which is disposed substantially vertical to said heat conducting wall,
- c) an fluid inlet for providing the cartridge with fluid,
- d) an fluid outlet for draining fluid or gas from the cartridge[.],
- e) a channel connecting inlet and outlet wherein said cartridge having a protrusion [(5)] such that the channel between fluid inlet and fluid outlet is longer than the shortest distance [Distance (D)] between fluid inlet and fluid outlet to allow flow-through-filling of the cartridge to avoid bubbles in a measuring section of the cartridge.

14. (Amended) [Cartridge according to] The cartridge of claim 13, having two opposing heat conducting walls.

15. (Amended) [Cartridge according to] The cartridge of claim 13 or 14, wherein the heat conducting wall is a foil with a thickness of less than 200µm.

16. (Amended) [Cartridge according to] The cartridge of claim 13 or 14, having two opposing walls from which at least one is a heat conducting wall and which form an angle of 3 to 8° with respect to each other.
17. (Amended) [Cartridge according to] The cartridge of claim 13, wherein the light transparent wall comprises a first section for transmitting light into the cartridge and a second section for transmitting light emerging from the cartridge.
18. (Amended) [Cartridge according to] The cartridge of claim 13, which is made from a body having at least one opening which is closed by a heat conducting foil.
19. (Amended) [Cartridge according to] The cartridge of claim 13, which is made from a frame which is closed by two opposing foils.
20. (Amended) [Cartridge according to] The cartridge of claim 13 having a thickness of [0,5] 0,5 to 5 mm.
21. (Amended) [Cartridge according to] The cartridge of claim 13, wherein [said channel has a width DL (lateral diameter) and a depth DV (vertical diameter) and wherein] the quotient of the maximal width [DL, max] of said channel and [DV] the depth of said channel is in the range of 1 to 10.
22. (Amended) [Cartridge according to] The cartridge of claim 21, wherein the depth [DV (vertical diameter)] of the channel is in the range of 0.5 to 5 mm.
23. (Amended) [Method] A method for thermocycling of fluids employing a system according to claim 1, [with] comprising the steps of
- filling the cartridge by a flow-through-process avoiding bubbles in a measuring section of the cartridge,
  - thermal cycling of fluid in the cartridge,

- transmitting light into the cartridge and
- detecting light emerging the cartridge.

24. (Amended) [Method according to] The method of claim 23 additionally comprising monitoring the light emerging the cartridge to monitor amplification of nucleic acids in the fluid during thermal cycling.

**Exhibit B**  
**Claims Pending After Entry of Amendment**

1. (Amended) A system for thermocycling of fluids in cartridges comprising
  - a) a cartridge with at least one heat conducting wall and at least one light transparent wall, the cartridge having a fluid inlet and an outlet which are connected by a channel,  
  
said cartridge having a protrusion such that the channel is longer than the shortest distance between the fluid inlet and fluid outlet to allow bubble-free flow-through filling of the cartridge,
  - b) a thermocycling unit in thermal contact with said heat conducting wall of said cartridge,
  - c) a light source for transmitting light into the interior of said cartridge through said light transparent wall of said cartridge which is arranged substantially perpendicular to said heat conducting wall,
  - d) a light detector for detecting light emerging from the interior of the cartridge through said light transparent wall,
  - e) a fluid providing unit coupled to an inlet of the cartridge for providing the cartridge with fluid by flow-through-filling.
2. (Amended) The system of claim 1, wherein the cartridge has a body comprising the light transparent wall and having at least one opening which is sealed by a foil providing said heat conducting wall.
3. (Amended) The system of claim 2, wherein the body is a frame which is sealed by two foils providing heat conducting walls.

4. (Amended) The system of claim 1 for conducting fluorescent measurements wherein the light detector detects fluorescent light emerging from the cartridge.
5. (Amended) The system of claim 1, wherein the thermocycling unit comprises at least one plate in thermal contact with the heat conducting wall of the cartridge.
6. (Amended) The system of claim 1, wherein the cartridge is wedge shaped and the thermocycling unit comprises a wedge shaped receiving section for receiving said wedge shaped cartridge.
7. (Amended) The system of claim 6, wherein the opposing walls forming the wedge shaped cartridge comprise opposing walls having an angle of 3 to 8° one to another.
8. (Amended) The system of claim 1, wherein said light transparent wall comprises a first section through which light is passed from the light source into the cartridge and a second section through which light is passed from the interior of the cartridge onto the light detector.
9. (Amended) The system of claim 8, wherein said first section is tilted with respect to the illumination beam axis so that the light is refracted towards the second section of said transparent wall.
10. (Amended) The system of claim 1 or 5, wherein said thermocycling unit comprises a plate in thermal contact with said heat conducting wall of the cartridge and which exerts pressure onto said wall.
11. (Amended) The system of claim 1, wherein the quotient of the maximal width of said channel and the depth of said channel is in the range of 1 to 10.
12. (Amended) The system of claim 1 or 11, wherein the depth of the channel is in the range of 0.5 to 5 mm.

13. (Amended) A cartridge for conducting thermal cycling of fluids, comprising
- a) a substantially planar and heat conducting wall,
  - b) a light transparent wall which is disposed substantially vertical to said heat conducting wall,
  - c) an fluid inlet for providing the cartridge with fluid,
  - d) an fluid outlet for draining fluid or gas from the cartridge,
  - e) a channel connecting inlet and outlet wherein said cartridge having a protrusion such that the channel between fluid inlet and fluid outlet is longer than the shortest distance between fluid inlet and fluid outlet to allow flow-through-filling of the cartridge to avoid bubbles in a measuring section of the cartridge.
14. (Amended) The cartridge of claim 13, having two opposing heat conducting walls.
15. (Amended) The cartridge of claim 13 or 14, wherein the heat conducting wall is a foil with a thickness of less than 200 $\mu$ m.
16. (Amended) The cartridge of claim 13 or 14, having two opposing walls from which at least one is a heat conducting wall and which form an angle of 3 to 8° with respect to each other.
17. (Amended) The cartridge of claim 13, wherein the light transparent wall comprises a first section for transmitting light into the cartridge and a second section for transmitting light emerging from the cartridge.



18. (Amended) The cartridge of claim 13, which is made from a body having at least one opening which is closed by a heat conducting foil.
19. (Amended) The cartridge of claim 13, which is made from a frame which is closed by two opposing foils.
20. (Amended) The cartridge of claim 13 having a thickness of 0.5 to 5 mm.
21. (Amended) The cartridge of claim 13, wherein the quotient of the maximal width of said channel and the depth of said channel is in the range of 1 to 10.
22. (Amended) The cartridge of claim 21, wherein the depth of the channel is in the range of 0.5 to 5 mm.
23. (Amended) A method for thermocycling of fluids employing a system according to claim 1, comprising the steps of
- filling the cartridge by a flow-through-process avoiding bubbles in a measuring section of the cartridge,
  - thermal cycling of fluid in the cartridge,
  - transmitting light into the cartridge and
  - detecting light emerging the cartridge.
24. (Amended) The method of claim 23 additionally comprising monitoring the light emerging the cartridge to monitor amplification of nucleic acids in the fluid during thermal cycling.

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5 System for thermocycling of fluids in cartridges

This invention is directed to a system for thermocycling fluids in cartridges to achieve an amplification and detection of nucleic acid sequences. A specific aspect of the present invention is that amplification and monitoring of the amplification process can be made  
10 simultaneously without changing the position of the cartridge. A further aspect of this invention is the complete and bubble free filling of cartridges with fluids for thermocycling. The monitoring of the amplification process may be used to quantify the starting concentration of a target nucleic acid.

15 An apparatus for performing nucleic acid amplifications in reaction cartridges is known from US 5,567,617. This U.S. patent is concerned with an invention for nucleic acid amplification in a flexible cuvette. For amplification this cuvette is placed within a heater having a thin heating element with a central window providing an optical passage. Such an embodiment has the disadvantage that heating and detection compete for free space in the  
20 lateral direction of the reaction cuvette. A further problem of the system used in US 5,567,617 is the flexible nature of the cuvette with fluid channels therein. Measures have to be taken to ensure that fluid communication within the cuvette is not obstructed when the cuvette is placed within the heater.

25 The present invention is directed to a system for thermocycling similar to the system described in US 5,567,617 but having the advantage that heating efficiency is not limited by free space needed for detection. A further advantage compared to US 5,567,617 is that a constriction of fluid passways within the cartridge is uncritical.

30 Document WO 98/38487 describes an assembly with a thermal sleeve for controlling the temperature within a fluid chamber. The assembly further comprises an optics for interrogation of the chamber content while the chamber is placed in the thermal sleeve.

The chamber disclosed however is designed to receive fluid by bottom up filling via a fluid port at the upper end of the chamber. Filling of such a chamber is uncritical if the inner diameter is large enough to allow fluid to enter without enclosure of air bubbles. Reduction of the diameter, however, is desirable to reduce for the internal distance between

5 temperature controlled walls to allow for sufficient heating and cooling rates of the fluid.

The aim of the present invention is to provide a system for rapid thermocycling of fluids in cartridges with on-line optical monitoring. A particular goal is to achieve rapid heating and cooling rates while avoiding the disturbance of optical measurements by bubbles enclosed

10 in the fluid.

This goal is achieved by a system with a thermocycling unit, a light source, a light detector, a fluid providing unit, and a cartridge in which thermocycling as well as detection can be conducted while the cartridge remains unchanged in position. Such a system allows

15 thermocycling with on-line optical monitoring. On-line monitoring means optical monitoring while temperature cycling is being performed. Furthermore the cartridge has a sufficiently small inner diameter between the temperature controlled walls to allow close temperature control of fluid in the cartridge. Filling of the cartridge is advantageously achieved by a flow-through process.

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The cartridge of the present invention has the shape of a thin plate. The two opposing larger walls are used for heat transfer and one or more walls substantially vertical thereto are used for transmitting light into the cartridge and for transmitting light to be detected out of the cartridge. This cartridge design ensures that the optical path and the path for heat exchange are spatially separated so that detection and heat transfer do not compete for

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space. The thickness of the cartridge is preferably in the range of 2.5 – 5mm and the area of each wall for heat transfer is preferably in the range of 0,1 – 4 cm<sup>2</sup>. Such a cartridge can be made from a body having a bottom wall and upstanding side walls and the body being closed by a top wall to form a close cartridge with a reaction chamber therein. A preferable embodiment of the cartridge is however made from a frame which provides the side walls of the cartridge and which is closed by a bottom and a top wall. It is particular preferred when top and bottom walls are foils with a thickness of less than 200µm. A cartridge in

accordance with the present invention may have a uniform thickness but it is however preferred when the heat conducting top and bottom walls form an angle of 3 to 8 degree with respect to each other. Such a wedge shaped cartridge has the advantage that it provides efficient heat transfer and easy handling when used in connection with a thermocycling unit having a receiving section of a respective wedge shape.

Cartridges of the present invention can be made from transparent plastics. Preferably an annular shaped frame with a wall thickness of 0,3 – 4 mm is provided to form the side walls of the cartridge. The frame can be made e.g. by injection molding from polymers as polyethylen or polypropylen. The frame is closed by foils forming top and bottom walls by heat sealing. Processes for sealing a polymer foil onto such a frame are well known in the art and will therefor not be discussed in detail herein. Heat sealing processes are e.g. described in: Polymere Werkstoffe: 3rd volume, Editor: Hans Batzer.

Stuttgart;New York: Thieme. Bd. 2. Technologie 1, 1984, pages 206-212;

Kunststoffverarbeitung; Editor: Otto Schwarz et al.; 4th revised edition Würzburg: Vogel, 1988, pages 193 – 206 and Kunststoff-Folien: Herstellung, Eigenschaften, Anwendung; Editor: Joachim Nentwig. München, Wien: Hanser, 1994, pages 88 – 93. Metallised multilayer foils can also be employed for sealing onto the frame.

As will become clearer below in connection with the filling process the cartridge is being made from materials with high surface tension or the surface tension of inner walls can be enhanced. Such an enhancement of surface tension can be achieved by adequate oxid coating or plasma treatment of the surface. The limiting surface tension value enabling bubble free filling, however, depends on the surface tension of the fluid.

As mentioned it is advantageous to employ cartridges with a small internal diameter between the heat controlled walls of the cartridge. It has shown that a diameter below approx. 5 mm allows close temperature control and thus high heating and cooling rates.

It should be noted that the interior of the cartridge may have fluid channels, as well as protrusions and recesses. Furthermore the used language "closed cartridge" does not

exclude fluid channels intersecting the walls of the cartridge which are used for bringing fluids into or out of the cartridge.

The thermocycling unit of the present invention comprises a heating section for  
5 establishing a thermal contact with the heat conducting walls of the cartridge. The heating section preferably comprises at least one plate which is brought into mechanical contact with the heat conducting wall of the cartridge and the plate itself being heated and cooled as necessary for the thermocycling process. This heating and cooling can be made by e.g. Peltier elements, bringing the plate into contact with hot and cold fluids or by heating with  
10 a resistor heater and cooling by blowing air onto the plate. Procedures and apparatuses for performing thermocycling by thermal contact with plates are well known in the art.

It should be understood, however, that other devices for heating and cooling the cartridges can be used without departing from the scope of the invention. It is only necessary that  
15 whatever device is used for heating and cooling the cartridges, be capable of reaching and sustaining the temperatures involved and achieve the desired temperature versus time profile. Thus, for purposes of nucleic acid amplification, such a device should be capable of cycling the temperature of the amplification reaction mixture between a denaturing temperature  $T_1$  (which can be in the range of about 80-105°C and preferably 90-100°C) and  
20 an annealing/extension temperature  $T_2$  (which can be in the range of about 30-90°C and preferably 50-70°C) where  $T_1 > T_2$  as is known to those skilled in the art.

To achieve a sufficient thermal contact between the cartridge and the heating section means can be provided which press one or two plates against the cartridge. Such means are  
25 e. g. described in US 5,567,617. In the context of the present invention it is however preferred to employ a heating unit having a receiving section of a wedge shaped recess. The receiving section may be formed by two walls which are inclined one to the other. A wedge shaped cartridge can be simply placed into such a wedge shaped receiving section and sufficient thermal contact between the walls of the receiving section and the heat  
30 conducting walls of the cartridge is automatically achieved by mechanical contact into which the respective walls come when the cartridge runs down into the receiving section.

The thermocycling unit further comprises a steering unit which steers the timely heating and cooling of the heater section. Such a steering section is for example described in EP B 0 236 069 which is hereby incorporated by reference. The present invention does not need a steering unit different to the one described in EP B 0 236 069 but timing, temperature  
5 profiles and the amount of heat exchanged with the cartridge has to be adapted to the specific needs.

The present invention involves nucleic acid amplification and the detection, monitoring and quantification of amplification products. In order to facilitate understanding of the  
10 amplification data collection and processing system of the present invention, a summary of nucleic acid amplification processes especially suited for use in conjunction with the invention will first be discussed.

Those of skill will recognize that the present invention requires amplification of the duplex  
15 form of nucleic acid. There exist well-known methods for amplifying nucleic acids. The means for amplification are not critical and this invention will work with any method where nucleic acid duplexes are generated. The various methods are reviewed in Bio/Technology 8:290-293, April 1990. They include, but are not limited to PCR, LCR, Q $\beta$  and 3SR. Although 3SR and Q $\beta$  do not involve thermal cycling, the result of their  
20 amplifications can be monitored by the fluorescence detecting arrangement discussed below and analyzed in accordance with the principles of the present invention. Each method is briefly described below.

PCR amplification of DNA involves repeated cycles of heat denaturing the DNA,  
25 annealing two oligonucleotide primers to sequences that flank the DNA segment to be amplified, and extending the annealed primers with DNA polymerase. The primers hybridize to opposite strands of the target sequence and are oriented so that DNA synthesis by the polymerase proceeds across the regions between the primers, each successive cycle essentially doubling the amount of DNA synthesized in the previous cycle. This results in  
30 the exponential accumulation of the specific target fragment, at a rate of approximately  $2^n$  per cycle, where n is the number of cycles. A complete review of this technology can be found in PCR Technology- Principles and Applications, Ed. Erlich H.A., Stockton Press,

Now York 1989. Taq DNA polymerase is preferred when PCR is used in conjunction with the present invention although this is not an essential aspect of the invention.

The ligase chain reaction is described in International Patent Application WO 89/09835.

- 5 The process involves the use of ligase to join oligonucleotide segments that anneal to the target nucleic acid. Ligase chain reaction (LCR) results in amplification of an original target molecule and can provide millions of copies of product DNA. Consequently, the LCR results in a net increase in double-stranded DNA. The present detection methods are applicable to LCR, as well as PCR. LCR typically requires some means for detecting the
- 10 product DNA such as an oligonucleotide probe. When used in conjunction with the disclosed methods for detecting amplification products, such means are unnecessary, and the LCR result is immediately detectable.

- Another amplification scheme, Q-beta replicase, exploits the use of the replicase from the
- 15 RNA bacteriophage QB. In this amplification scheme, a modified recombinant bacteriophage genome with a sequence specific for the targeted sequence is initially ligated to the nucleic acid to be tested. Following enrichment of the duplexes formed between the bacteriophage probe and the nucleic acid in a sample, QB replicase is added, which, upon recognizing the retained recombinant genome, begins making a large number of copies.
- 20 The QB system does not require primer sequences and there is no heat denaturation step as with the PCR and LCR amplification systems. The reaction occurs at one temperature, typically 37°C. The preferred template is a substrate for the QB replicase, midvariant-1 RNA. A very large increase in the templates is achieved through the use of this system. A review of this amplification system can be found in International Patent Application WO
- 25 87/06270 and in Lizardi et al., 1988, Bio/Technology 6:1197-1202.

- The 3SR system is a variation of an in vitro transcription-based amplification system. A transcription-based amplification system (TAS) involves the use of primers that encode a promoter sequence as well as a complementary sequence to the target strand to generate
- 30 DNA copies of a target strand and the production of RNA copies from the DNA copies with an RNA polymerase. See, e.g., Example 9B of U.S. Patent No. 4,683,202 and

European Patent Application EP-A-0 310,229. The 3SR System is a system which uses three enzymes to carry out an isothermal replication of target nucleic acids.

The system begins with a target of singlestranded RNA to which a T7 RNA DNA primer is bound. By extension of the primer with reverse transcriptase, a cDNA is formed, and RNaseH treatment frees the cDNA from the heteroduplex. A second primer is bound to the cDNA and a doublestranded cDNA is formed by reverse transcriptase treatment. One (or both) of the primers encodes a promoter, e.g., the promoter for T7 RNA polymerase, so that the double-stranded cDNA is a transcription template for RNA polymerase.

Transcription competent cDNAs yield antisense RNA copies of the original target. The transcripts are then converted by the reverse transcriptase to double-stranded cDNA containing double-stranded promoters, optionally on both ends in an inverted repeat orientation. These DNAs can yield RNAs, which can reenter the cycle. A more complete description of the 3SR system can be found in Guatelli et al., 1990, Proc. Natl. Acad. Sci. USA 87:1874-1878, and European Patent Application EP-A-0 329 822.

According to the present invention, nucleic acid amplification is monitored by detecting fluorescence emitted when a fluorescent dye such as an intercalating fluorescent dye, provided in the reaction mixture, binds with the double-stranded nucleic acid during each annealing/extension phase as the mixture is cycled between two temperatures (thermal cycling). An increase in fluorescence indicates a positive amplification of target nucleic acid. Suitable intercalating agents or dyes include, but are not limited to ethidium bromide, propidium bromide, proflavine, acridine orange, acriflavine, fluorcoumarine, ellipticine, daunomycin, chloroquine, distamycin D, chromomycin, homidium, mithramycin, ruthenium polypyridyls, anthramycin, methidium bromide, 2-[2-(4-hydroxyphenyl)-6-benzimidazole-6-(1-methyl4-piperazyl) benzimidazole trihydrochloride and the like.

Fluorophores and DNA binding chromophores described in the art are suitable for use in the 5' to 3' nuclease assay disclosed in U.S. Patent No. 5,210,015 are also useful in the present invention. Suitable donor fluorophores and quenchers are chosen such that the emission spectrum of the donor fluorophore overlaps with the absorption spectrum of the



quencher. Ideally, the fluorophores should have a high Stokes shift (a large difference between the wavelength for maximum absorption and the wavelength for maximum emission) to minimize interference by scattered excitation light.

- 5 Suitable labels which are well known in the art include, but are not limited to, fluorescein and derivatives such as FAM, HEX, TET, and JOE; rhodamine and derivatives such as Texas Red, ROX, and TAMRA; Lucifer Yellow, and coumarin derivatives such as 7-Me2N-coumarin-4-acetate, 7OH-4-CH3-coumarin-3-acetate, and 7-NH2-4-CH3coumarin-3-acetate (AMCA). FAM, HEX, TET, JOE, ROX, and TAMRA are marketed by Perkin
- 10 Elmer, Applied Biosystems Division (Foster City, CA). TEX-as Red and many other suitable compounds are marketed by Molecular Probes (Eugene, OR). Examples of chemiluminescent and bioluminescent compounds that may be suitable for use as the energy donor include luminol (aminophthal-hydrazide) and derivatives, and Luciferases.
- 15 The optics of a system in accordance with the present invention comprises a light source and a light detector. With the system absorption or scattering measurements with the fluid within the cartridge can be performed. It is however preferred to use this system for fluorescent measurements where light is transmitted into the interior of the cartridge to initiate fluorescence emission which is detected by the light detector. The light source may
- 20 comprise semi-conductor light sources as well as halogen lamps or other embodiments. Within the spirit of the present invention the light is transmitted into the cartridge through a second light transparent wall of the cartridge which is substantially perpendicular to the wall for heat transfer. Due to the flat shape of the cartridge the second light transparent wall has a width of only 0,5 to 5 mm in one dimension. It is therefor preferred to employ
- 25 beam shaping optics cooperating with the light source to introduce light through this restricted window. Such beam shaping optics may include apertures, lenses and fibre optics. For fluorescent measurements it is necessary to stimulate fluorescent dyes with light of a wavelength within the absorption spectrum of the dye. It is normally desired to suppress background radiation caused by light emission from other sources than the
- 30 fluorescent dye. In many embodiments it is furthermore desirable to perform fluorescent measurements with two or more dyes within the same reaction volume. In these cases it is necessary to restrict the bandwidth of the light for illumination. This can be done by using

light sources having a narrow bandwidth as for e.g. LED's or by using light sources having a broad bandwidth in connection with suitable filters.

A system of the present invention further comprises one or more light detectors for  
5 detecting light emerging from the interior of the cartridge through the second light  
transparent wall. Suitable light detectors are semiconductor detectors as photodiodes or  
photomultipliers. As already mentioned it is desirable to suppress background signals and  
therefore detection should be limited to the emission band of the fluorescent dye to be  
detected. This can be achieved by wavelength filters or by spectral separation of the light  
10 with a spectrometer. Within the present invention it is preferred to detect two or more  
fluorescent dyes within the same cartridge by separate detection of the emitted fluorescent  
radiation from the dyes. Advantageously the dyes are also stimulated separately with  
suitable light sources.

15 The light detector of the present invention may cooperate with light directing means as  
fibreoptics, lens systems and so on.

The cartridge of the present invention is used as a thermocycling cavity for fluids and it  
therefore has an inlet for providing the cartridge with fluid. Optionally the cartridge may  
20 have an outlet for draining fluid from the cartridge. It is however preferred in some modes  
of use to have a disposable cartridge without an outlet for liquid. Such a cartridge can be  
discarded together with its content after use. The inlet and the optional outlet are preferably  
channels through the body or through the frame of the cartridge. As already mentioned  
body or frame are made mostly incompressible so that the fluid channels are not obstructed  
25 when pressure is applied to the cartridge in order to achieve a thermal contact with the  
heating unit. A system in accordance with the present invention comprises a fluid  
providing unit which is coupled to the inlet of the cartridge. Such a fluid providing unit  
may be a pipetting unit or an internal fluid channel of the system from which fluid is  
pressed into the cartridge. The system optionally comprises a fluid receiving unit which is  
30 coupled to an outlet of the cartridge to receive fluid from the cartridge. Such a fluid  
receiving unit is necessary if the cartridge has to be emptied or if different fluids have to be  
processed within the same cartridge. In preferred embodiments the cartridge is however

discarded together with the fluid therein after single use. Such embodiments do not need a fluid receiving unit but only an outlet to drain gas when the cartridge is filled with fluid.

Cartridges in accordance with the present invention a preferably filled by the so called flow-through-filling. Flow-through filling means that fluid is introduced via an inlet and fills the inner space of the cartridge directly adjacent the inlet. Introduction of further liquid continuously enlarges the filled space until a desired degree of filling is achieved. In this process the fluid bolus is never released from the inlet during filling as it is the case for bottom-to-top-filling as described in WO 98/38487. To allow for a flow-through-filling process the inner geometry of the cartridge, respectively the channel connecting inlet and outlet is important. For thermocycling cartridges it is desirable to have a large contact area of fluid with the thermally controlled walls. The dimension of the channel which controls the contact area will be denoted  $D_L$  (lateral diameter) and the internal distance between the thermally controlled walls  $D_V$  (vertical diameter). The larger the quotient  $D_L/D_V$  the more efficient is heat control as well as the risk that bubbles are enclosed during filling. It has shown that optimal quotients  $D_L/D_V$  are in the range of 1 to 10.

Bearing in mind that the risk of bubble formation increases with increasing lateral diameter the quotient should be calculated employing the largest vertical diameter ( $D_V, \max$ ) of the channel, wherein the diameter is measured vertical to the flow direction.

Other factors as surface tension (of wall and fluid), viscosity of the fluid, capillary forces and filling rate also will influence the filling process. Said fluid channel, however does not necessarily have a unique shape at each section. It has shown advantageous to employ a curved channel so that the length  $L$  of the channel is larger than the geometric distance  $D$  between inlet and outlet. Such a design can efficiently be generated by a protrusion projecting into the interior of the cartridge as shown in figure 1.

The cartridge may also have a space for receiving gases which are set free during heating of the fluid. This space is arranged in a section of the cartridge which does not interfere with optical measurement.

The present invention is further described in more detail with the regard to the following figures:

- Figure 1: Cartridge in top view partially filled with fluid
- 5 Figure 2: Cartridge in top view with light sources and detector
- Figure 3: Light source module
- 10 Figure 4: Raytrace diagram with cartridge having an oblique window
- Figure 5: Fluorescence signal during thermocycling
- Figure 6: System for thermocycling in a cartridge within a metal block thermocycler,  
15 integrating light sources and light detector.
- Figure 7: System for thermocycling with wedge shaped cartridge
- Figure 8: Filling process of cartridge shown in figure 1.

20

Figure 1 shows a cartridge (1) for thermocycling of fluids in top view. The cartridge has a body (3) with a cavity (2) therein. The cartridge body has been molten from a solid polypropylene block. In the region of the cavity material was removed until a cell bottom of 200µm thickness had been achieved. (In serial production the cartridge can be produced  
25 more efficiently by injection molding.) Into the polypropylene block has also been molten an inlet (10) to receive fluid and an outlet (11) to vent air from the cavity during filling. The body of the cartridge shown in figure 1 has been closed by welding a sealing foil of 40µm thickness onto the cartridge body. Figure 1 shows a preferred shape of the cavity (2) with a protrusion (5) in form of a nose reaching into the cavity. The protrusion (5) ensures  
30 that the cavity can be filled completely with fluid without enclosure of air bubbles.

The protrusion modifies the geometry of the cartridge so that the largest lateral diameter  $D_{L, \max}$  is reduced as well as the quotient  $D_{L, \max}/D_V$  ( $D_V$  is the distance between the heat controlled walls; i.e. the thickness of the fluid in the cartridge). In the shown experimental setup  $D_{L, \max}$  was 4.0 mm and  $D_V$  was 1.5 mm resulting in a quotient of 2.7.

5

The size of protrusion (5) has to be adapted to this specific situation and depends on cavity thickness, viscosity of the liquid, surface tension of bottom and top wall of the cartridge as well as size and shape of the cavity. It has been found that the effect of the protrusion is to avoid a fluidic shortcut between inlet and outlet. In this spirit the protrusion directs the fluid on a path (L) which is longer than the shortest distance (D) between inlet and outlet. In Figure 1 there have been shown several fluid paths by dotted lines. It has been found to be advantageous if the quotient of the shortest L divided by D is two or more. Figure 1 furthermore shows a preferred embodiment with respect to the location of inlet and outlet on the same side of the cartridge. With this arrangement it is possible to locate fluid connections on the same side and make connection to an apparatus easier. A disposal of inlet and outlet on the same side is also advantageous in that this side may be located upside within the system during filling, cycling and measurement. By this arrangement air bubbles remaining occasionally in the cavity or being created during heating of the cartridge can be eliminated through the inlet or the outlet port. Figure 1 also shows an advantageous shape of the cavity adjacent inlet and outlet. As can be seen the walls, (7', 7'', 7''') form an angle with the inlet and outlet of approximately 130°. A preferred range of this angle is 100 - 150° which has shown to avoid empty spots when filling the cavity with fluid. A further aspect of the present invention which can be seen in figure 1 are the oblique windows (4, 4'). Light is irradiated into the cavity perpendicular to surfaces (8, 8') of the cavity and is detected by schematically shown detector (20). The irradiating light is being refracted by the oblique surfaces (4, 4') in a direction towards the detector. Due to this arrangement the generation of fluorescent light can be directed to a central portion of the cavity which is closer to the detector in order to increase the measurement sensitivity.

30

Figure 2 shows a schematic drawing of a cartridge in combination with light sources (30, 30', 30'', 30''') and a detector (20). As can be seen the focal point of the light sources is being disposed in the centre of the cavity and the focal points are mostly coincident. The

detector (20) is disposed beneath the detection window of the cartridge to detect fluorescent light from the centre of the cavity. With the setup of figure 2 it is possible to monitor the fluorescence of four different fluorescent dyes. Each of the light sources is chosen to specifically stimulate one of the fluorescent dyes. By subsequent activation of the light sources the amount of each fluorescent dye can be monitored by detection of fluorescent radiation with the detector.

Figure 3 shows a light source module which can be advantageously used within the present invention. The light source module comprises a semiconductor light source (31) a wavelength selection filter (32) and an optical output power monitor (33). The output power monitor comprises a beam splitter (33a) to extract a portion of the light from the light path and a detector (33b) to detect the extracted light. The amount of light detected is used to steer the current applied to the semiconductor light source so as to generate a constant and specific output. The light source module of figure 3 further comprises a beam shaper (34) in form of a lens. Advantageously the light emitting surface of the semiconductor light source is imaged by the lens into the centre of the cartridge.

Figure 4 shows a raytrace of a system employing a cartridge with an oblique window. As can be seen the light generated by light source (30) is imaged by a ballshape lens (35) onto an oblique window (4) of the cartridge. Due to this rangement the light is refracted in direction of the detector (20).

Figure 5 depicts a fluorescence over time diagram which was measured with the system according to the present invention. The abscissa shows the number of the measurement and the ordinate shows fluorescence intensity in arbitrary units. Measurements were taken after each denaturation, elongation cycle of the polymerase chain reaction. A cartridge (1) as shown in figures 1 and 6 has been introduced and fixed in a holder as shown in figure 6. The holder with the cartridge had been integrated into a thermocycler unit. Illumination optics with simple beam shaping optics and detection optics have been used for quantitative fluorescence measurement. PCR runs (HCV-control with Mastermix,  $5 \times 10^3$  initial copies) with the following protocol have then been performed: 120 cycles, denaturation temperature  $T_{\text{denat}} = 94^\circ\text{C}$ , annealing temperature  $T_{\text{anneal}} = 60^\circ\text{C}$ , temperature

ramp time  $t_{\text{ramp}}$  approx. 20 s, temperature plateau  $t_{\text{plateau}}$  approx. 26 s, total process time  $t_{\text{tot}}$  approx. 3 h. The experimentally measured fluorescence signal vs. number of measurement is plotted in Fig. 5 (solid line). For comparison, the fluorescence signal of an amplification within a vessel has been measured with the same PCR protocol. The result is also shown in Fig. 5 (dotted line). The decreased fluorescence signal of the cartridge (approx. factor 2) is a result of the beam shaping optics used for measurement. This optics introduces an illumination power loss of approximately 30 %.

Figure 6 shows a cartridge of the present invention in the cavity of a metal block for thermocycling. Within the metal block there are integrated light sources and a light detector. For thermocycling the closure (41) can be screwed onto the metal block (40) so as to achieve an optimum thermal contact between the cartridge and the metal block. The metal block itself is provided with Peltier elements for heating and cooling.

Figure 7 shows an advantageous system in accordance with the present invention. The cartridge shown is a wedge shaped embodiment having a larger thickness on the side of inlet and outlet. The system is provided with a wedge shaped receiving unit comprising of Peltier elements (40') forming an angle one to the other so as to receive the wedge shaped cartridge. With this embodiment it is possible to achieve an intensive thermal contact between the cartridge and the heating unit by simply inserting the cartridge between the Peltier elements (40'). This figure shows that the optical path and the path for heat exchange are spatially separated so that detection and heat transfer do not compete for space.

Figure 8 shows the filling of the cartridge of figure 1 with fluid. Fluid is introduced through inlet (10) and fills the cartridge region directly adjacent the inlet (picture a)). Further introduction of fluid enlarges the filled region as can be seen in figures 8b) and c). This flow-through-filling process provides a bubble free filling of the cartridge.

Art:34

# Claims

- 1 System for thermocycling of fluids in cartridges comprising
  - a) a cartridge with at least one heat conducting wall and at least one light transparent wall, the cartridge having a fluid inlet and an outlet which are connected by a channel,

said cartridge having a protrusion (5) such that the channel is longer than the shortest distance (D) between fluid inlet and fluid outlet to allow bubble-free flow-through filling of the cartridge
  - b) a thermocycling unit in thermal contact with said heat conducting wall of said cartridge (1),
  - c) a light source (30) for transmitting light into the interior of said cartridge through said light transparent wall of said cartridge said light transparent wall being arranged substantially perpendicular to said heat conducting wall,
  - d) a light detector (20) for detecting light emerging from the interior of the cartridge through said light transparent wall,
  - e) a fluid providing unit coupled to an inlet of the cartridge for providing the cartridge with fluid by flow-through-filling. .
2. System according to claim 1, wherein the cartridge has a body comprising the light transparent wall and having at least one opening which is sealed by a foil providing said heat conducting wall.
3. System according to claim 2, wherein the body is a frame which is sealed by two foils providing heat conducting walls.
4. System according to claim 1 for conducting fluorescent measurements wherein the light detector detects fluorescent light emerging from the cartridge.



5. System according to claim 1, wherein the thermocycling unit comprises at least one plate (40) in thermal contact with the heat conducting wall of the cartridge.
6. System according to claim 1, wherein the cartridge is wedge shaped and the thermocycling unit comprising a wedge shaped receiving section for receiving said wedge shaped cartridge.
7. System according to claim 6, where the opposing walls forming the wedge shaped cartridge comprise opposing walls having an angle of 3 to 8° one to another.
8. System according to claim 1, wherein said light transparent wall comprises a first section through which light is passed from the light source into the cartridge and a second section through which light is passed from the interior of the cartridge onto the light detector.
9. System according to claim 8, wherein said first section is tilted with respect to the illumination beam axis so that the light is refracted towards the second section of said transparent wall.
10. System according to claim 1 or 5, wherein said thermocycling unit comprises a plate (40) in thermal contact with said heat conducting wall of the cartridge and which exerts pressure onto said wall.
11. System according to claim 1, wherein said channel has a width  $D_L$  (lateral diameter) and a depth  $D_V$  (vertical diameter) and wherein the quotient of maximal width  $D_{L, \max}$  and  $D_V$  is in the range of 1 to 10.
12. System according to claim 1 or 11, wherein the depth  $D_V$  (vertical diameter) of the channel is in the range of 0.5 to 5 mm.

A4.34

13. Cartridge for conducting thermal cycling of fluids, comprising
- a) a substantially planar and heat conducting wall,
  - b) a light transparent wall which is disposed substantially vertical to said heat conducting wall,
  - c) an fluid inlet for providing the cartridge with fluid
  - d) an fluid outlet for draining fluid or gas from the cartridge.
  - e) a channel connecting inlet and outlet wherein said cartridge having a protrusion (5) such that the channel between fluid inlet and fluid outlet is longer than the shortest Distance (D) between fluid inlet and fluid outlet to allow flow-through-filling of the cartridge to avoid bubbles in a measuring section of the cartridge.
14. Cartridge according to claim 13, having two opposing heat conducting walls.
15. Cartridge according to claim 13 or 14, wherein the heat conducting wall is a foil with a thickness of less than 200µm.
16. Cartridge according to claim 13 or 14, having two opposing walls from which at least one is a heat conducting wall and which form an angle of 3 to 8° with respect to each other.
17. Cartridge according to claim 13, wherein the light transparent wall comprises a first section for transmitting light into the cartridge and a second section for transmitting light emerging from the cartridge.
18. Cartridge according to claim 13, which is made from a body having at least one opening which is closed by a heat conducting foil.
19. Cartridge according to claim 13, which is made from a frame which is closed by two opposing foils.
20. Cartridge according to claim 13 having a thickness of 0,5 to 5 mm.

A4.34

21. Cartridge according to claim 13, wherein said channel has a width  $D_L$  (lateral diameter) and a depth  $D_V$  (vertical diameter) and wherein the quotient of maximal width  $D_{L, \max}$  and  $D_V$  is in the range of 1 to 10.
22. Cartridge according to claim 21, wherein the depth  $D_V$  (vertical diameter) of the channel is in the range of 0.5 to 5 mm.
23. Method for thermocycling of fluids employing a system according to claim 1, with the steps
- filling the cartridge by a flow-through-process avoiding bubbles in a measuring section of the cartridge,
  - thermal cycling of fluid in the cartridge
  - transmitting light into the cartridge
  - detecting light emerging the cartridge.
24. Method according to claim 23 additionally monitoring the light emerging the cartridge to monitor amplification of nucleic acids in the fluid during thermal cycling.

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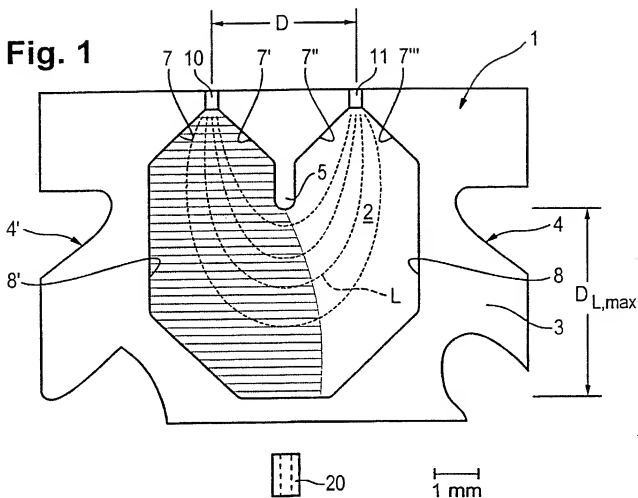
(54) Title: SYSTEM FOR THERMOCYCLING OF FLUIDS IN CARTRIDGES

(57) Abstract: System for thermocycling of fluids in cartridges comprising a thermocycling unit in thermal contact with a first substantially planar and heat conducting wall of a cartridge, a light source for transmitting light into the interior of said cartridge through a second light transparent wall of said cartridge which is arranged substantially perpendicular to said first wall, a light detector for detecting light emerging from the interior of the cartridge through said second wall and a fluid providing unit coupled to an inlet of the cartridge for providing the cartridge with fluid and an outlet of the cartridge to drain gas when the cartridge is filled with fluid. The invention further concerns a cartridge for conducting the thermal cycling of fluids.

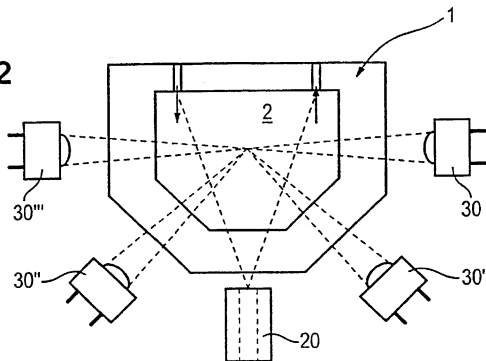
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**Fig. 1**



**Fig. 2**



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Fig. 3

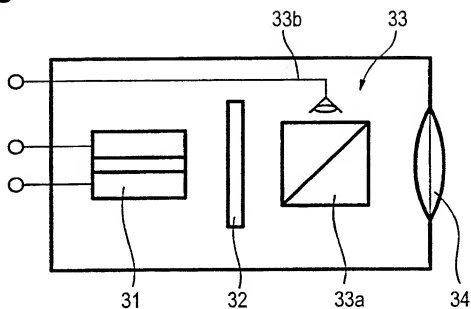
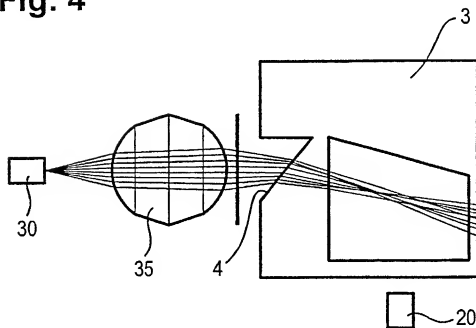
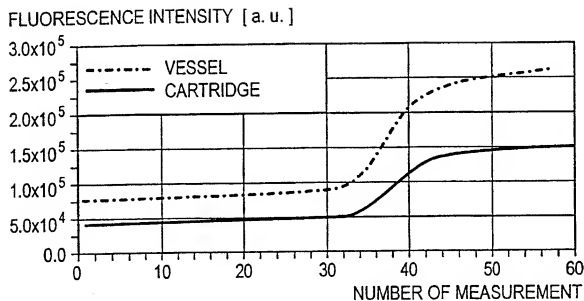
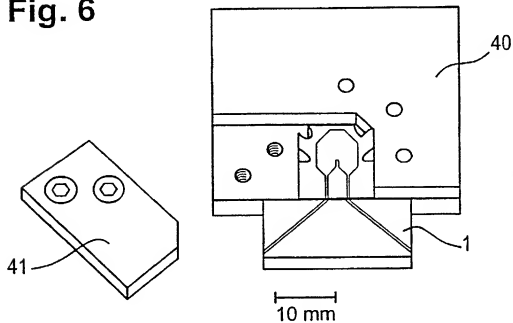


Fig. 4

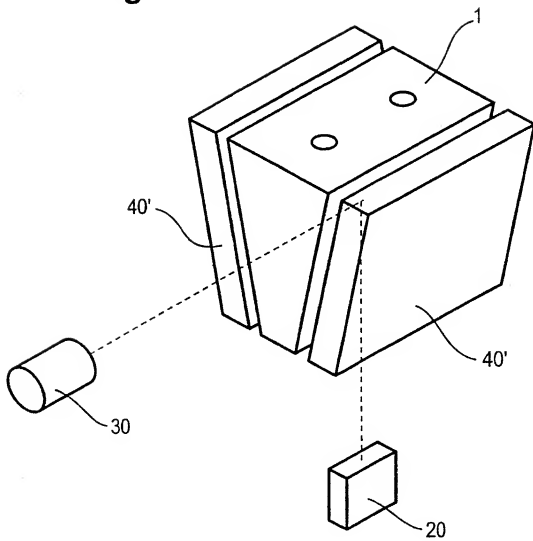


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**Fig. 5****Fig. 6**

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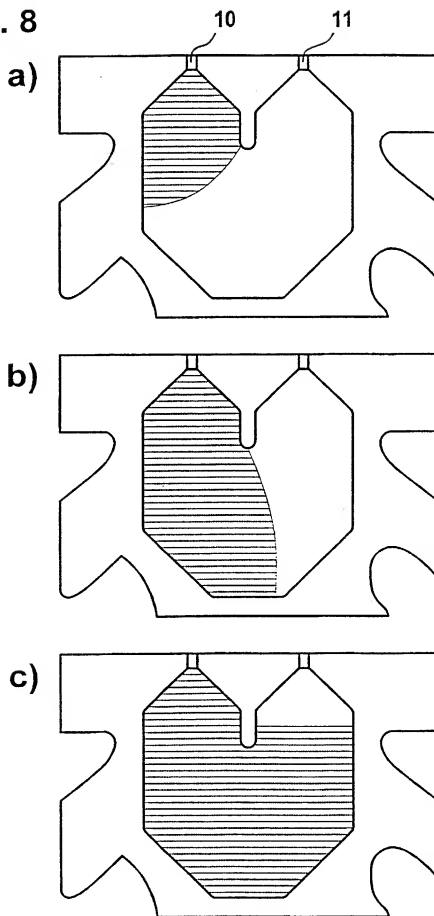
Fig. 7





5 / 5

Fig. 8





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## DECLARATION FOR NON-PROVISIONAL PATENT APPLICATION\*

As a below named inventor, I hereby declare that:

My residence, post office address and citizenship are as stated below at 201 et seq. beneath my name.

I believe I am the original, first and sole inventor if only one name is listed at 201 below, or an original, first and joint inventor if plural names are listed at 201 et seq. below, of the subject matter which is claimed and for which a patent is sought on the invention entitled

## SYSTEM FOR THERMOCYCLING OF FLUIDS IN CARTRIDGES

and for which a patent application:

□ is attached hereto and includes amendment(s) filed on (if applicable)

■ was filed in the United States on February 28, 2002 as Application No. 10/070,343 (for declaration not accompanying application)

■ with amendment(s) filed on (if applicable)

■ was filed as PCT international Application No. PCT/EP00/08587 on 2 September 2000 and was amended under PCT-Article 19 on (if applicable)

I hereby state that I have reviewed and understand the contents of the above identified application, including the claims, as amended by any amendment referred to above.

I acknowledge the duty to disclose information known to me to be material to patentability as defined in Title 37, Code of Federal Regulations, §1.56.

I hereby claim foreign priority benefits under Title 35, United States Code, §119(a)-(d) of any foreign application(s) for patent or inventor's certificate listed below and have also identified below any foreign application for patent or inventor's certificate having a filing date before that of the application on which priority is claimed:

EARLIEST FOREIGN APPLICATION(S), IF ANY, FILED PRIOR TO THE FILING DATE OF THE APPLICATION			
APPLICATION NUMBER	COUNTRY	DATE OF FILING (day, month, year)	PRIORITY CLAIMED
EP 99117506.8	Europe	4 September 1999	YES <input checked="" type="checkbox"/> NO
			YES NO
			YES NO

I hereby claim the benefit under Title 35, United States Code, §119(e) of any United States provisional application(s) listed below.

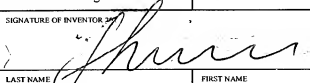
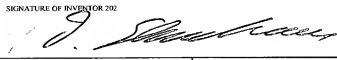
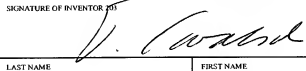
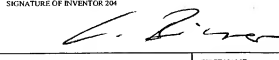

PROVISIONAL APPLICATION NUMBER	FILING DATE

I hereby claim the benefit under Title 35, United States Code, §120 of any United States application(s) listed below and, insofar as the subject matter of each of the claims of this application is not disclosed in the prior United States application in the manner provided by the first paragraph of Title 35, United States Code §112, I acknowledge the duty to disclose information known to me which is material to patentability as defined in Title 37, Code of Federal Regulations, §1.56 which became available between the filing date of the prior application and the national or PCT international filing date of this application:

NON-PROVISIONAL APPLICATION SERIAL NO.	FILING DATE	STATUS		
		PATENTED	PENDING	ABANDONED

\* for use only when the application is assigned to a company, partnership or other organization.

I hereby declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under Section 1001 of Title 18 of the United States Code and that such willful false statements may jeopardize the validity of the application or any patent issuing thereon.

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	SIGNATURE OF INVENTOR 204 			DATE <u>July 2, 02</u>
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	SIGNATURE OF INVENTOR 205 			DATE <u>July 2, 2002</u>